

A KURSUS 2014

Diagnostisk Radiologi : ” Fysik og Radiobiologi ”

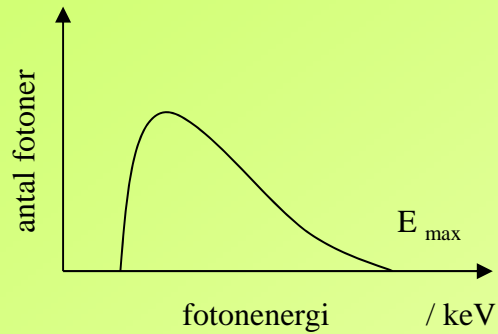
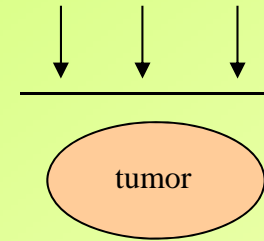
STRÅLINGSKVALITET

Erik Andersen, ansvarlig fysiker

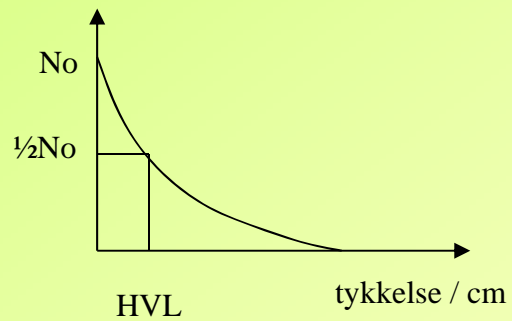
CIMT Medico Herlev, Gentofte, Glostrup Hospital

”Definition” af strålingskvalitet :

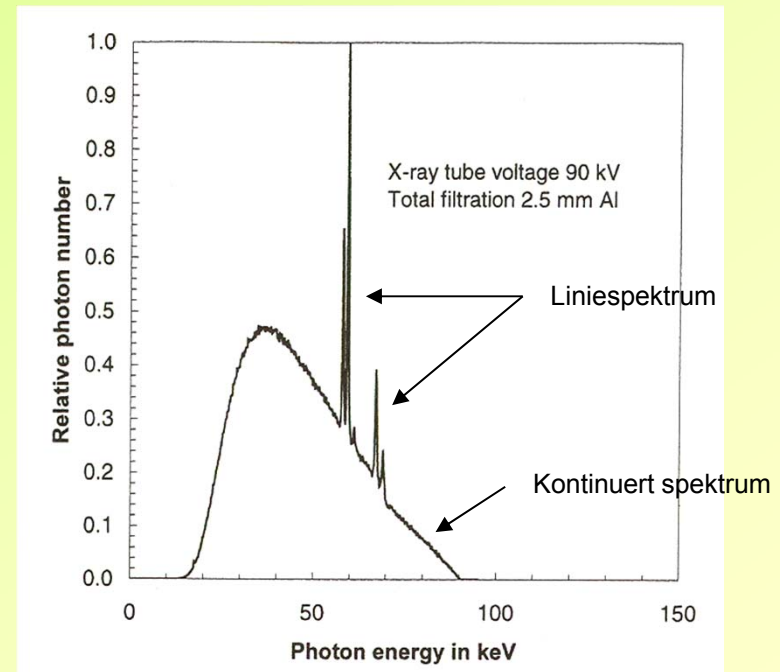
- Røntgenstrålingens ”gennemtrængningsevne” :
- Røntgenstrålingens spektrale Energifordeling :



- HVL halvværdilag :

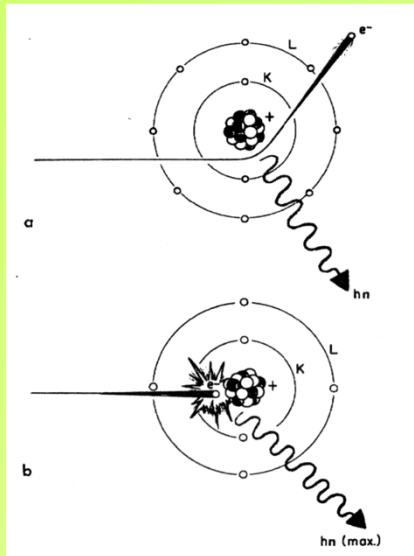


Røntgenspektrum :



Dannelse af røntgenspektret :

Kontinuert spektrum :
Bremsestråling



Fotonens energi : $E_{foton} = h \cdot f$

h = Plancks konstant = $6,63 \cdot 10^{-34}$ J·s

f = frekvensen

Linie spektrum :
Karakteristisk stråling

$$E_{foton} = E_n - E_m = h \cdot f$$

K_{α} , K_{β} linier

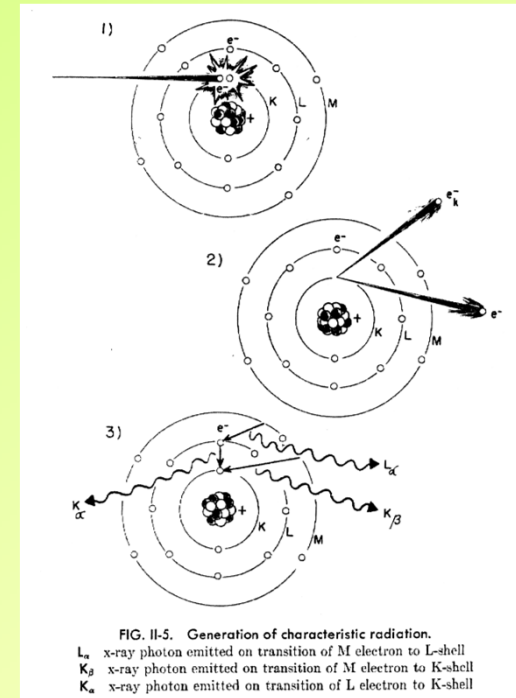
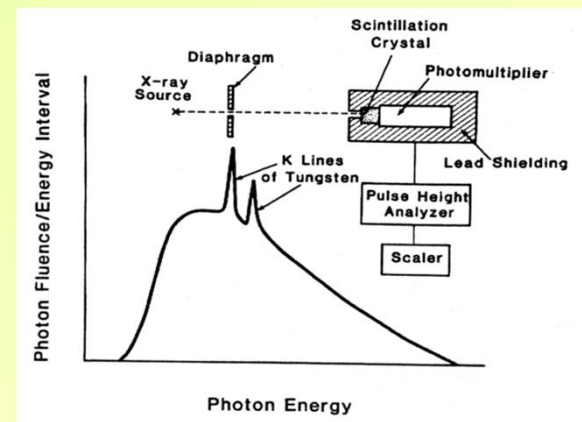


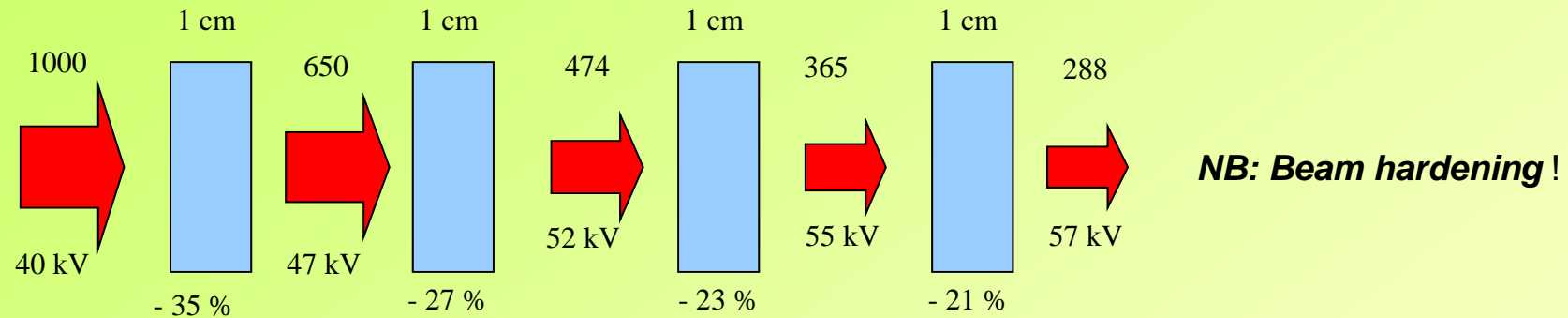
FIG. II-5. Generation of characteristic radiation.
 L_{α} x-ray photon emitted on transition of M electron to L-shell
 K_{β} x-ray photon emitted on transition of M electron to K-shell
 K_{α} x-ray photon emitted on transition of L electron to K-shell

”Måling” af røntgenspektret :



Attenuation af røntgenstråling / røntgenspektrum:

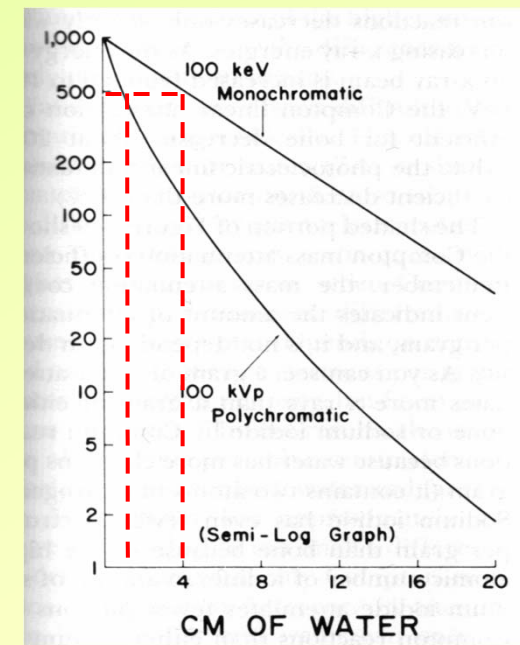
Eks.: 100 kVp ~ ca. 40 keV i middelenergi af røntgenstrålingen.



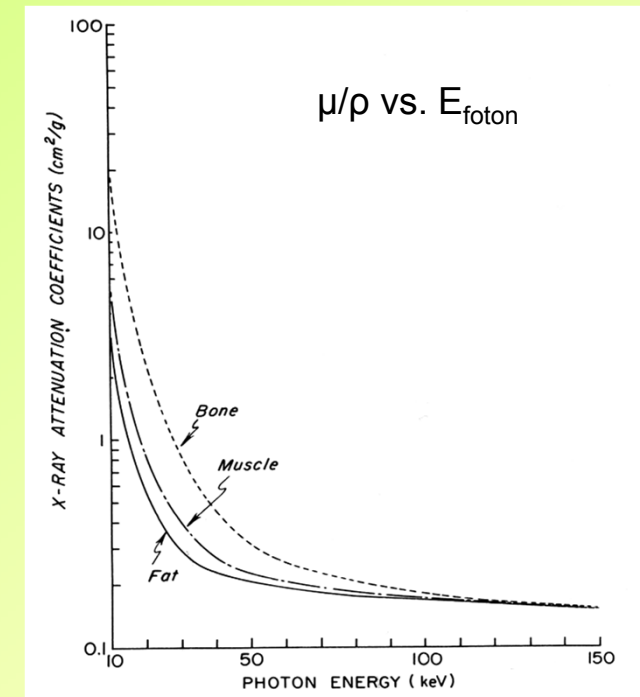
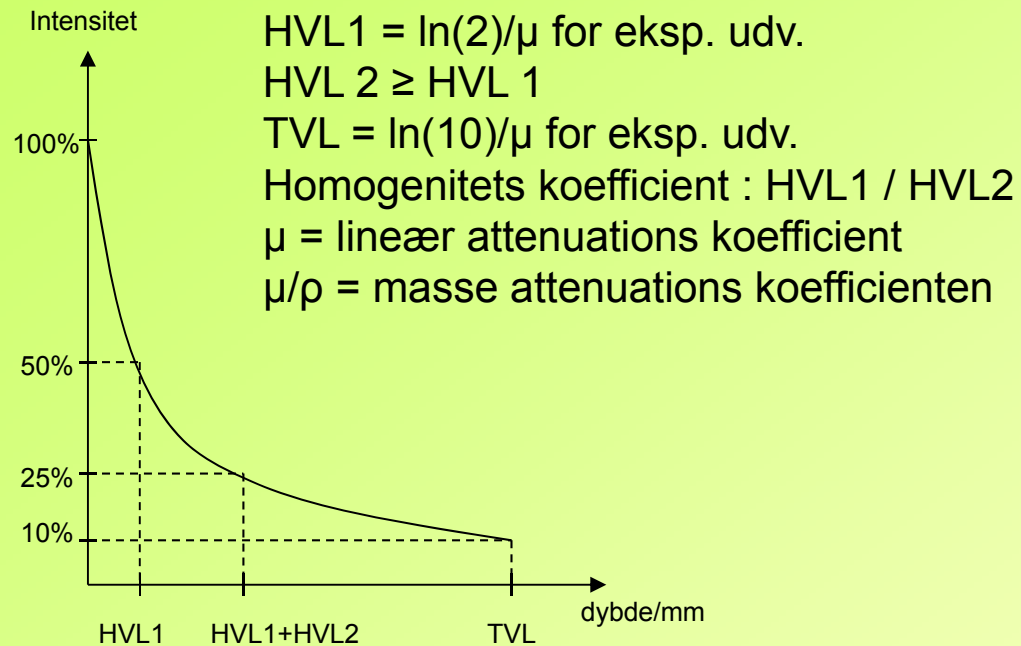
NB: Kun for monoenergetisk stråling er attenuationen i stof eksponentielt aftagende (dvs. en ret linie i semi-log. koordinatsystem)

HVL_{poly} er mindre end HVL_{mono} inden for de første cm.

For større dybder er HVL_{poly} næsten lig med HVL_{mono}

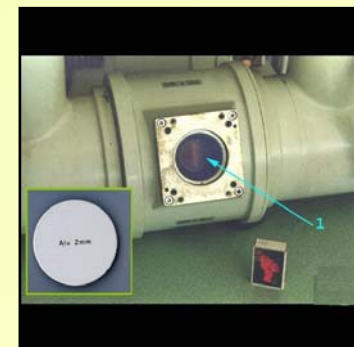


Halvværdilag HVL :



Filtrering af røntgenstrålingen :

- Røntgenspektrets form ændres ved filtrering med f.eks. Al og Cu.
- mindsker strålingsintensiteten i den lavenergetiske del af spektret
 - beamhardening (spektrets middelenergi E_{mid} øges)
 - mindsker derved hudosis til patienten
 - ændrer kontrasten i røntgenbilledet



Filtrering af røntgenstrålingen :

Indre filtre : ~ 0,5 – 1,0 mm Al
Be vindue, olie, glaskappe m.m.

Ydre filtre :

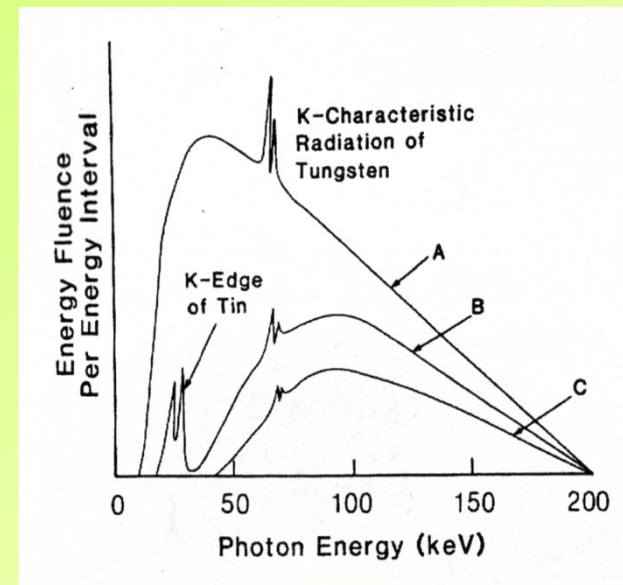
kurve A : Al

kurve B : Sn + Al

kurve C : Sn + Cu + Al

Røntgenspektrets middelenergi øges
A → B → C. (*Beamhardening*).

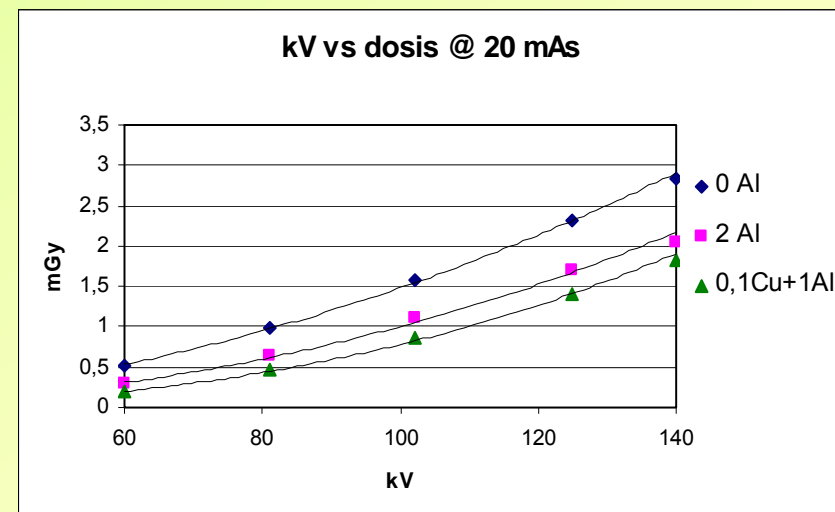
Krav : Totalfiltrering i røret $\geq 2,5$ mm Al



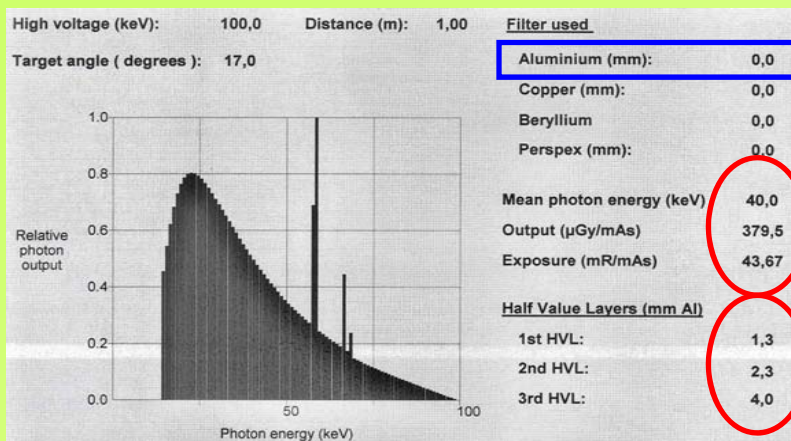
Dosis output fra røntgenrøret :

Høj filtrering :

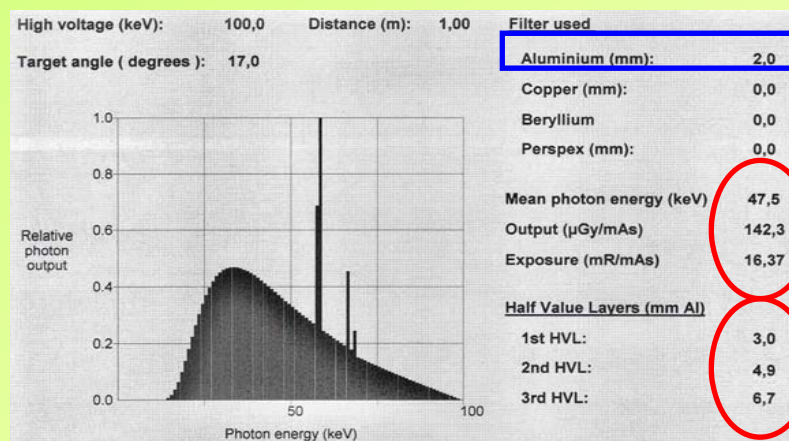
- mindsker dosis output fra røret
- øger belastningen af røret
- mindsker levetiden af røret



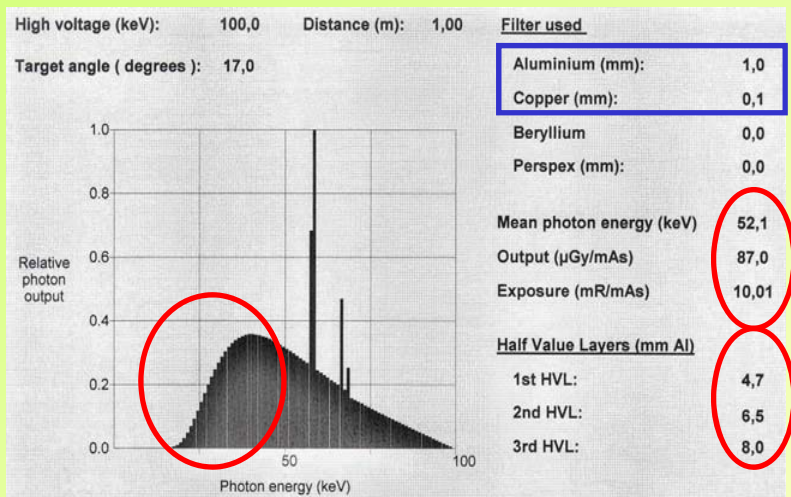
Filtrering : 0 Al



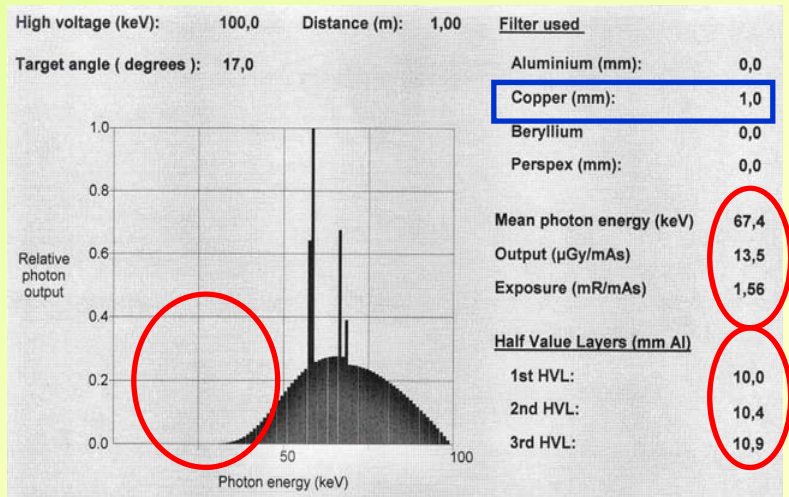
Filtrering : 2 Al



Filtrering : 1 Al + 0,1 Cu

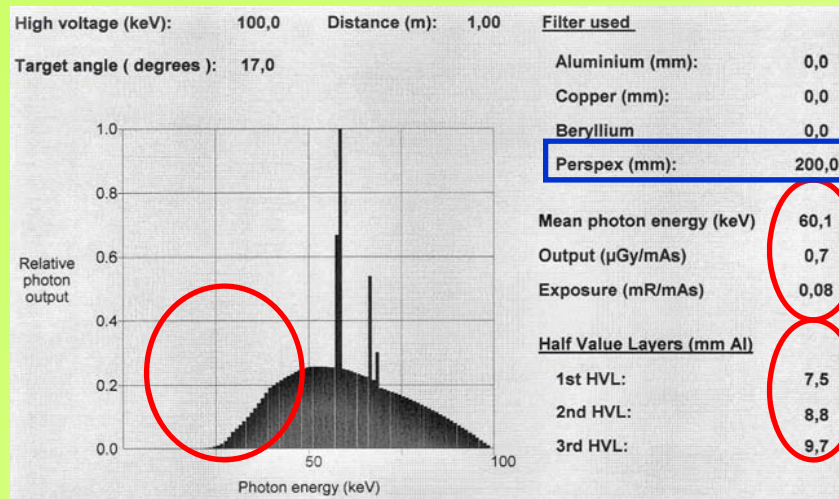


Filtrering : 1 Cu



NB : Reduktion af huddosis til patienten

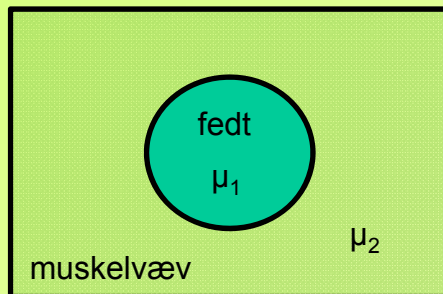
Filtrering : 20 cm PMMA



Typiske filter kombinationer i røntgenrør :

- 0 Al, 2 Al, 0,1Cu+1Al, 0,2Cu+1Al
- 0 Al, 0,1Cu, 0,2Cu, 0,3Cu

Filtrering og kontrast :



Attenuation

$$I = I_0 \cdot \exp(-\mu \cdot x)$$

Eks.: 100 kVp , fedtvæv – muskelvæv kontrast

Filter	E_{mean}	$\mu_1 \text{ cm}^{-1}$	$\mu_2 \text{ cm}^{-1}$	$C = (I_1 - I_2)/I_2$
0 Al	40 keV	0,2276	0,2819	5,58 %
2 Al	47,5 keV	0,2082	0,2486	4,12 %
0,1Cu+1Al	52,1 keV	0,1987	0,2328	3,47 %
1 Cu	67,4 keV	0,1814	0,2063	2,52 %

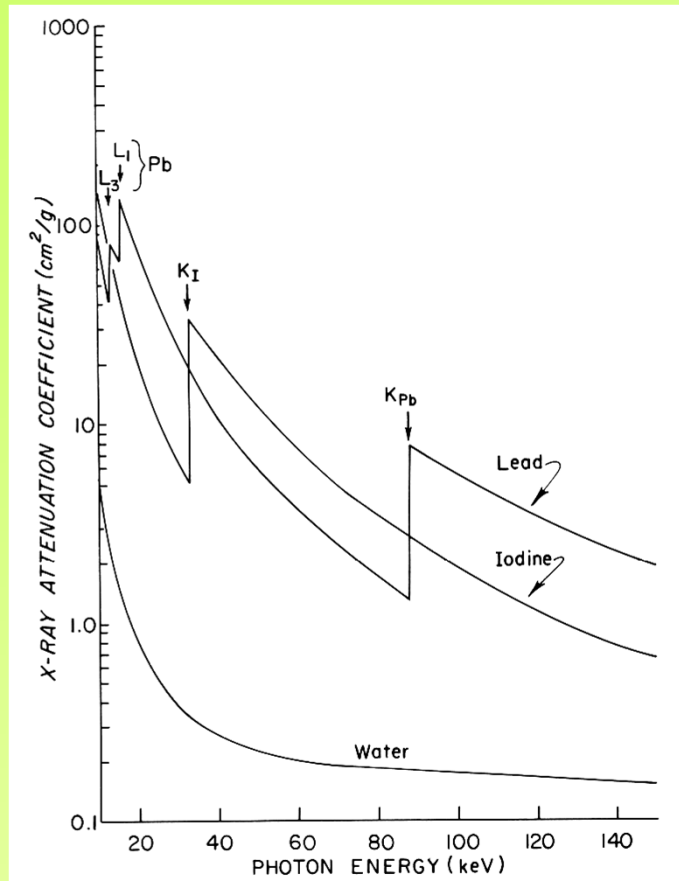
Kontrasten C mindskes med øget filtrering

Spredt stråling mindsker kontrasten yderligere

Kontraststoffer :

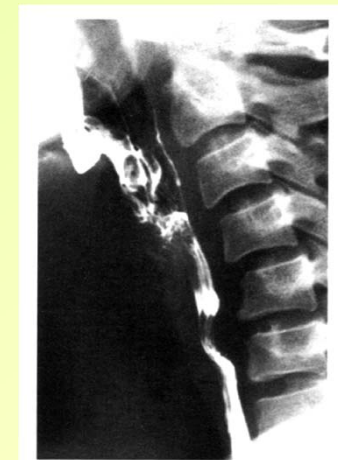
K – kanter

Masse attenuations koefficienter μ/ρ



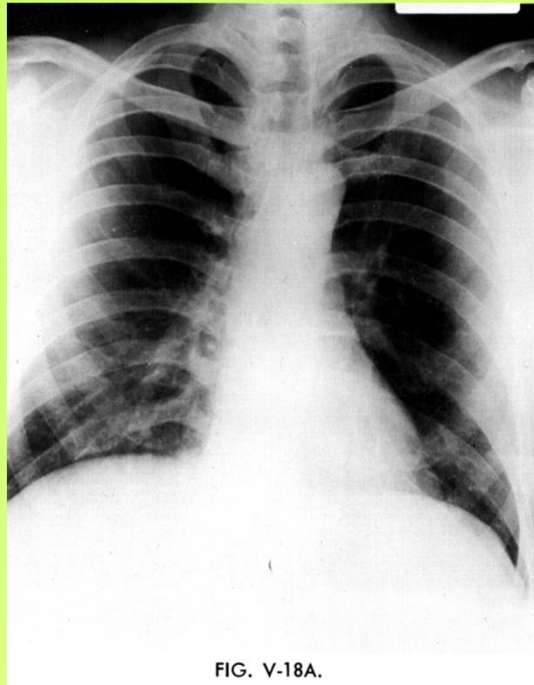
Grundstof	Symbol	A	K – kant (keV)
Aluminum	Al	13	1,6
Iod	I	53	33,17
Barium	Ba	56	37,45
Wolfram	W	74	69,5
Bly	Pb	82	88,0

Røntgenbilleder : Barium Ba

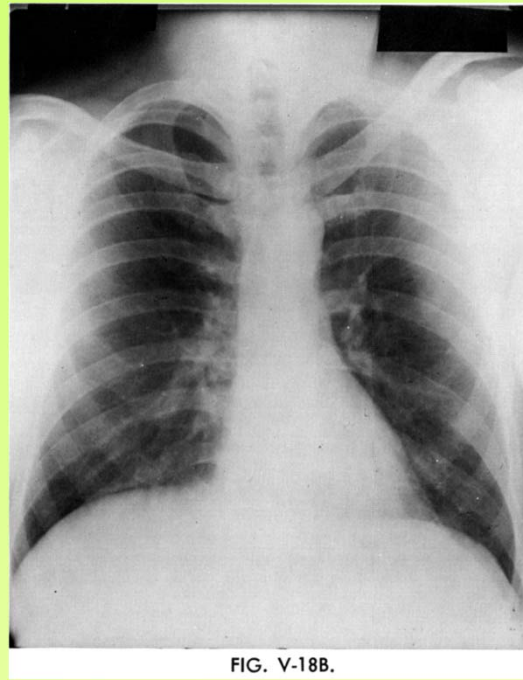


Pharynx, lateral X-r

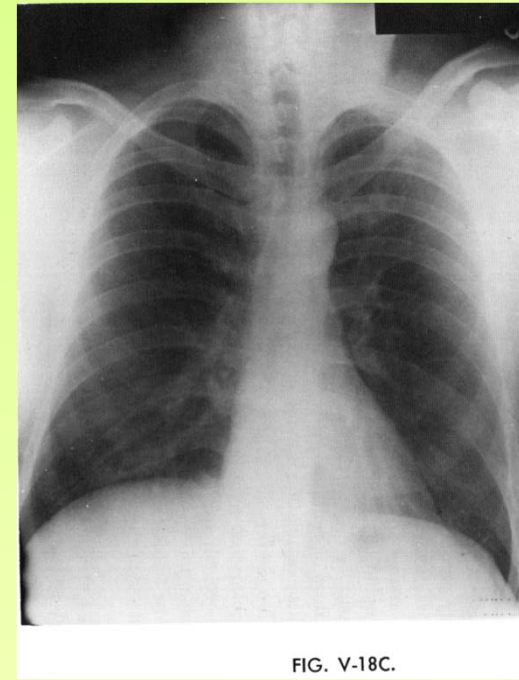
Strålekvalitet og billedkvalitet :



75 kV, 16mAs



100 kV, 4,8 mAs



150 kV, 2,0 mAs

NB : AEC Automatic Exposure Control benyttet !

The End !

